

Supplementary material

ImFCS: A software for Imaging FCS data analysis and visualization

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1. Overview and Functions of the software

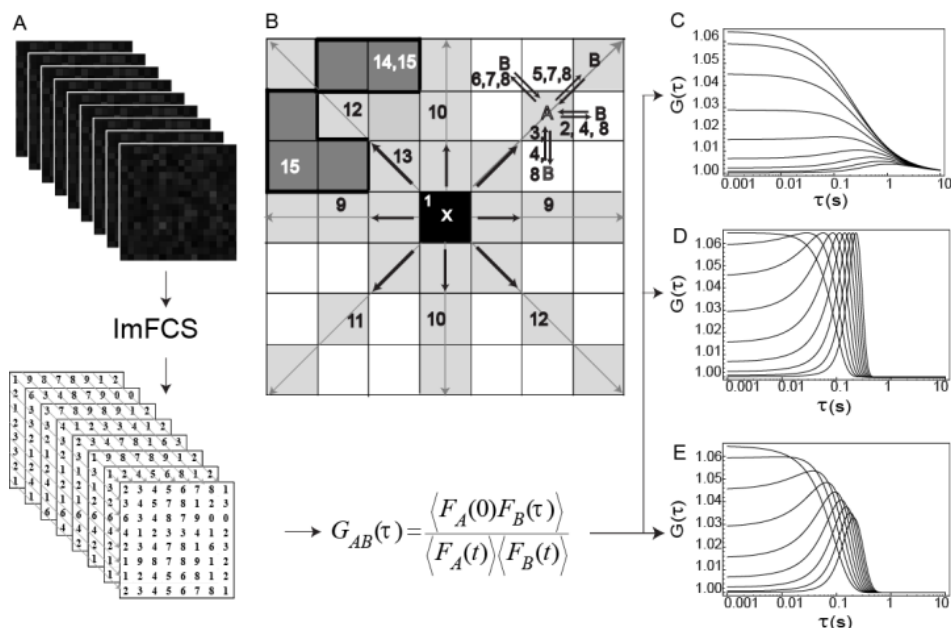


Fig. S1: The raw data to ImFCS is a set of images whose intensities values are read and correlated as seen in A. The data can be fitted upon correlation to yield diffusion coefficients and flow velocities. B is a schematic of all the correlations that can be performed by ImFCS. Autocorrelation is denoted by 1. 2, 3 and 4 perform ACCF along the horizontal and/or vertical directions. ACCF along the trailing and/or leading diagonals are denoted by 5, 6 and 7. Option 8 calculates all the ACCF described above. 9, 10, 11 and 12 are cross-correlations of the center pixel with all other pixels along the horizontal, vertical, leading and trailing diagonals respectively. 13 is the cross-correlation of all the pixels in a rectangular region surrounding the center pixel with the center pixel. 14 allows the user to choose a small rectangular region in the image and perform correlations of all the pixels in the chosen region. The user has the option to cross-correlate continuous pixel combination of varied shapes as depicted in 15. C, D and E are simulations of typical correlation curves obtained as output from the software using option 9. C, D and E are sets of cross correlation curves calculated with increasing distances of separation between them for a diffusion process with a D of $1 \mu\text{m}^2/\text{s}$, for a flow process at a speed of $10 \mu\text{m}/\text{s}$ and a combination of both the above processes respectively. The cross-correlations were calculated between pixels of increasing distances of separation along the direction of flow.

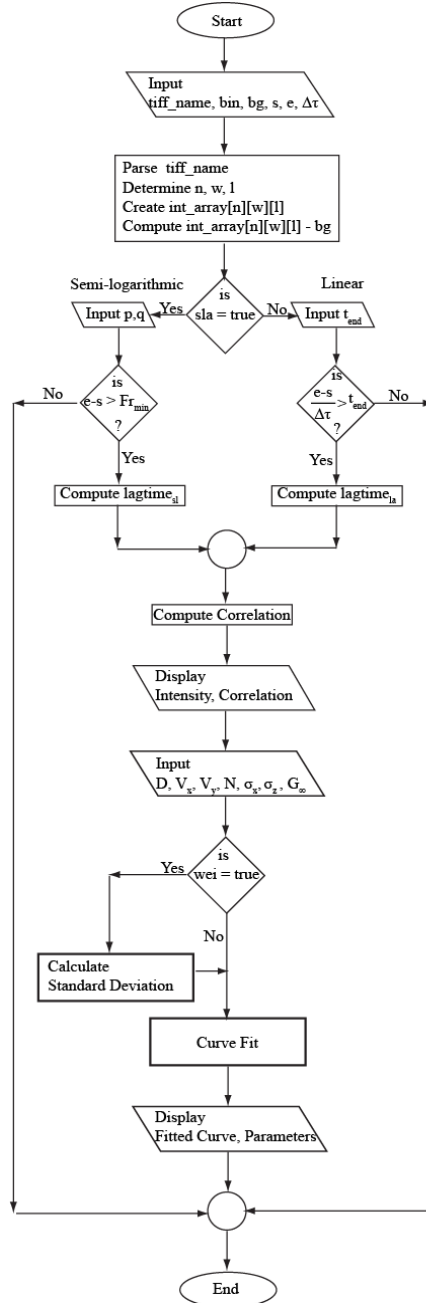


Fig. S2: A flowchart of ImFCS. The name of the tif file containing the stack is the input to the program. It is not necessary to correlate the entire tif stack, since the initial few frames acquired by few camera models may show an unstable background due to camera artifacts. Hence the user can specify the start and end of the frames to be correlated through s and e . The background is subtracted from the intensity file. sla is a Boolean variable which is used to decide the correlator architecture. There is a checkpoint to ensure there is sufficient number of frames to calculate the correlations. The correlations are computed. wei is a Boolean variable which determines the type of fitting. The standard deviation is computed only in the case of weighted fitting. The curves are fit and the fitted curves and parameters are provided as output from the program.

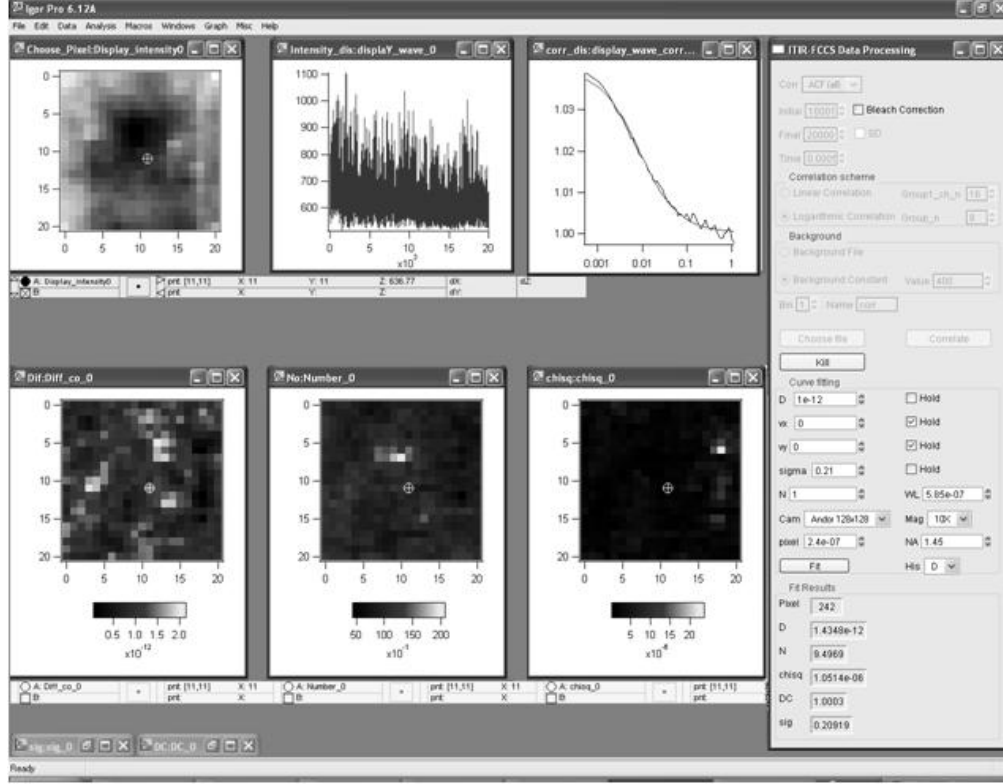


Fig. S3: A screen shot of ImFCS analyzing a diffusion process. The data has been correlated and fitted and quantitative parameters (D , N , χ^2) are rendered on the screen.

2. Details of the software

2.1 Software requirements

The function calculating the correlation described above was programmed in C++ using Microsoft Visual Studio .net 2003(Redmond, WA, USA). This program is controlled using Igor Pro 6.0 as front end by reprogramming the above program using the external operation (XOP) tool kit provided by Igor Pro. XOPs were used instead of using Igor procedures because XOPs in C++ were much faster in performing “number-crunching operations” [1]. The source code is available with the package and the user is free to modify it. If necessary, the user can include newer fitting models. The program can be adapted for using Igor Pro in any other operating system or any other front end display software or both. In the former case, it has to be kept in mind that Igor Pro handles strings differently from many other programming languages like C, C++ etc since the strings in Igor Pro are not null terminated. The null character has to be manually added to the name of the tif file while being passed to the correlation function for calculation.

2.2 Details of the XOP

The XOP serves to transmit the parameters from Igor Pro to the C++ function calculating the correlations. The parameters which are transferred are the name of the stack file, the binning value, the minimum value to be subtracted as background, correlator architecture parameters and the arrays which contain the positions of the pixels to be cross-correlated. The

generalized function calculates the cross-correlation which could be adapted for autocorrelation as well. The XOP which transfers the name of the tif file to the program is an adaptation of the example XOP-xstrcat() provided by Igor Pro. In brief, Igor Pro transfers controls to XOPEntry() function in C++ .net2003 program which in turn transfers the control to a function which opens the specific tif file for parsing.

2.3 Parsing the tiff file structure

Any tiff file has an “image file header” (IFH) at the beginning. In the program, the IFH is read to determine the byte order. The byte order is of two types, “little endian” and “big endian”. The memory in any computer is organized as a series of words. Byte order is the sequence of storing bits in these words. In the “little endian” configuration, the byte order is from the least significant bit to the most significant bit and vice versa. The first two bytes in the IFH indicate byte order. This program works only on “little endian” format and is verified before execution of the rest of the program. Generally images acquired using Macintosh operating systems are stored as “big endian” and those from Windows are stored as “little endian”. Any stack acquired in “big endian” can be converted to “little endian” by open source image processing software like ImageJ [2].

The IFH contains the magic number [magic number = 42] in the next two bytes. These two bytes are read and the program continues execution if and only if the value read in these two bytes is the same as the magic number. The next two bytes indicate the location of the first “image file directory” (IFD) which locates the first frame in the tiff file.

Each frame is identified by its IFD which determines the location in the file. The present specification of tiff files allows multiple IFD per tiff file to facilitate the creation of multi-plane tiff files. Each IFD is an array of values and also contains the location of the subsequent IFD. The last IFD stores the location of the next IFD as “0” indicating the end of the stack. The IFDs are read until the value of “0” is reached in order to determine the number of frames (n) in the particular tiff file. The tags ImageWidth (w) and ImageLength (l) are read in order to determine the size of each frame. Tiff allows images of different sizes to present in a single multi-plane tiff file. The software implicitly assumes that the frames in the stack are of the same dimensions. The n, w and l values are used to define an intensity array which stores the intensity values of each pixel in the stack of files. This array serves as the input for the function which calculates the correlation using the intensity values.

The tag BitsPerSample (b) is used in order to determine the amount of bytes allocated for each pixel in the image. The tag StripOffsets stores the location at which the intensity values corresponding to the particular IFD is stored. The pointer in the program assigns $w \times l \times b / 8$ bytes to a temporary array and $w \times l$ values are read beginning from the position pointed by StripOffsets and stored corresponding to a particular n in the intensity array. This procedure is repeated for all the frames and the complete intensity array corresponding to the chosen tiff file is created.

2.4 User Interactive Correlation functions

The software allows the user to draw regions on the average intensity map allowing the user to select regions where the autocorrelation needs to be performed. This is programmed using the marquee option in Igor Pro. A marquee is any outline drawn using the mouse on an image. Getmarquee() function allows one to retrieve the co-ordinates of the vertices of the drawn outline so that only the pixels within these vertices are correlated. This feature of the software restricts the user to draw rectangular regions on the graph. The software possesses an additional option which allows the user to cross-correlate two polygonal shapes on the plot. The user is provided an option to draw on the average intensity plot for both the regions. While the user is drawing on the image, all other functions and buttons are disabled. Once the

user finishes the closed polygon (checked by the fact that the user should end the polygon at the point it was started), the FindPointsinPoly() function is invoked which identifies all the pixels which are within these two regions. The cross-correlation is calculated and displayed on the screen. The FindPointsinPoly function invokes the Graphics Device Interface (GDI) component of the Windows Application Programming Interface's (API). The GDI contains the PtInRegion() function which determines whether the pixels lie within the drawn polygon.

2.5 Calculation of the correlation

The summation is implemented using a “nested for loop” with k and l as the counters. The arrays storing F_A and F_B are allocated memory dynamically using malloc() for every value of l since the arrays are reduced in dimension by a factor 2 after every iteration due to the summing up of adjacent values. The program accepts only even integers for p . In case, the user enters an odd number, it is incremented by 1.

2.6 Output Parameters

The software provides an average intensity plot as an output. The user has the option to move the cursor on this plot and display the intensity at any particular pixel in the adjacent window. Upon correlation, the autocorrelation curve is displayed in an adjacent window. The autocorrelation and the intensity trace get updated when the cursor is moved in the image plot. After curve fitting, the fitting parameters are also displayed as images. When the cursor is moved on any of the above said images, the autocorrelation and intensity traces get updated and the corresponding fit values along with the pixel position is displayed in the window. This operation is performed synchronously by monitoring the cursor movement using “hook functions” described flow.

2.7 Hook functions

The cursor movement is intercepted by a “hook function” which determines the position of the cursor on the image. Igor Pro manual defines window hook functions as, “A window hook function is a user-defined function that receives notifications of events that occur in a specific window” [1]. The hook function in the software receives information about the movement of the cursor in the window which displays the average intensity value of the stack. It is programmed to follow the cursor since it provides the flexibility to the user to use the keyboard or mouse to move the cursor. The position is transferred to other functions which move the cursors on other plots to the same position. The corresponding intensity trace and autocorrelation curve is displayed along with updating the values of fitting parameters corresponding to the position of the cursor. The entire operation is performed in a synchronous manner.

2.8 Fitting Algorithm

The user is provided the option of fitting all the pixels in the image or fit only part of them by choosing a sub-rectangular region in the image. The Levenberg-Marquardt algorithm is used for non-linear least squares fitting for minimizing the reduced chi-squared χ^2_{red} [3-6]. The standard error of the mean or the standard deviation ($\sigma_{i,data}$) is used for weighting in the calculation of χ^2_{red} . For data, in which $\sigma_{i,data}$ is not available, the program performs unweighted non-linear least square fitting by assuming the weights to be 1. The major advantage of using weighted fits is that data points of different precision are handled differently. If the standard deviation is not the same across the entire set of data points to be

fitted, then weighted least square fitting is beneficial. In a typical correlation curve, the standard deviation varies with lag time since each point is calculated as an average from a different number of time points [7]. The fitting is performed without the value of $G(\tau = 0)$ since this value is affected by the shot noise of the detector. The open source code for the Levenberg-Marquardt algorithm was available from [8] and was modified to include weighted least square fitting. The software also provides options to perform fitting by using the curve fitting tool box in Igor Pro (described in Sec. 7).

The other modification made in the source code was to incorporate conditions in which the user was provided the flexibility to fix any fitting parameter if necessary. In general, there may be r fitting parameters in any expression, but from prior knowledge, the user could have access to some of the values, hence the user has the flexibility to fix the value of k known fitting parameters and fit the rest $r-k$ parameters. The advantage of using χ_{red}^2 is that the value is normalized to the degrees of freedom. Therefore χ_{red}^2 is close to 1 for a good fit. $\chi_{red}^2 > 1$ might indicate two things, the model is an inappropriate one to fit the data or it indicates that the standard error of the mean is underestimated. $\chi_{red}^2 < 1$ indicates that the fact that the standard error of the mean is over estimated or the data is overfitted by the model [9].

2.8.1 Calculating the weight factor

The standard error of the mean ($\sigma_{i,data}$) can be evaluated in 3 different ways, i) reduced Koppel's method, ii) calculation of $\sigma_{i,data}$ while calculating the correlation and iii) by estimating the standard deviation from the variation of correlations of multiple, non-overlapping subsets of the data set [7].

Koppel [10] derived an analytical expression for the error in autocorrelation functions. It has been derived for an exponential signal and it is pointed out by the author that the expression is "expected to be qualitatively correct for others". It is to be noted that, since the expression is derived for an exponential signal, which is a monotonically decreasing signal, this expression should not be used for cross-correlations which exhibit a peak and hence are not monotonically decreasing. It has been observed that Koppel's expression for standard deviation is a very good approximation of SD at smaller times but fails at longer times [7, 11, 12]. This led to the development of modified Koppel's formula. Koppel's formula will in general exhibit a minimum, SD_{min} , at an intermediate lagtime $\tau_{SD,min}$ and will then rise with increasing lagtime. This however, is not observed in the data in which the SD is found to be for $\tau > \tau_{SD,min}$. Therefore in the modified Koppel's formula the value of SD is fixed to SD_{min} for all $\tau > \tau_{SD,min}$. In our experience this give χ_{red}^2 values close to 1. The expressions for calculations are given in the supplement in Eqs. [S8] and [S9]. In the second option, the necessary calculations to get an experimental estimate of the SD is performed alongside the correlations. The formulae to calculate the standard deviation using this method is given as Eqs. [S10] and [S11] in the supplement. The last method to compute the SD is by splitting the original intensity file in several non-overlapping stacks for each of which the correlations are calculated. The SD and standard error for each point in the ACF can then be calculated from the variation of the multiple correlations.

2.8.2 Comparison of the three methods to determine the correlation

The advantage of using methods other than Koppel's formula is that they are calculated from the raw data and are free from any underlying assumptions. But this increases the computation time as the standard deviation is also calculated while calculating the correlation mean. In the case of splitting a stack, the number of frames used in calculating individual correlations to be averaged is reduced by at least a factor of 10. Hence this method is recommended only if there is sufficiently large number of stacks. Koppel's method has the disadvantage that a good estimate of N is necessary since Koppel's method requires the user to supply the value of N in the expression. Hence the user has to choose the method based on the constraints during the calculation.

3. Fitting model

3.1 Fitting model for ITIR-FCCS and IVA-FCCS

Two fitting models are included in the software to fit the data obtained above and to extract the parameters. The generalized fitting model for cross-correlation for square regions separated by r_x and r_y in the x and y axes respectively, for TIRF based camera FCS, for diffusion and flow processes [13] is given by

$$G_{df}(\tau) = G_{\infty} + \frac{1}{4Na^2} \times \quad [S1]$$

$$\left(\frac{2\sqrt{D\tau + \sigma^2}}{\sqrt{\pi}} \left(e^{-\frac{(a+r_x-v_x\tau)^2}{4(D\tau + \sigma^2)}} + e^{-\frac{(a-r_x+v_x\tau)^2}{4(D\tau + \sigma^2)}} - 2e^{-\frac{(r_x-v_x\tau)^2}{4(D\tau + \sigma^2)}} \right) \right.$$

$$\left. -2(r_x - v_x\tau) \operatorname{erf}\left(\frac{r_x - v_x\tau}{2\sqrt{D\tau + \sigma^2}}\right) + (a + r_x - v_x\tau) \operatorname{erf}\left(\frac{a + r_x - v_x\tau}{2\sqrt{D\tau + \sigma^2}}\right) \right.$$

$$\left. + (a - r_x + v_x\tau) \operatorname{erf}\left(\frac{a - r_x + v_x\tau}{2\sqrt{D\tau + \sigma^2}}\right) \right)$$

$$\left(\frac{2\sqrt{D\tau + \sigma^2}}{\sqrt{\pi}} \left(e^{-\frac{(a+r_y-v_y\tau)^2}{4(D\tau + \sigma^2)}} + e^{-\frac{(a-r_y+v_y\tau)^2}{4(D\tau + \sigma^2)}} - 2e^{-\frac{(r_y-v_y\tau)^2}{4(D\tau + \sigma^2)}} \right) \right.$$

$$\left. -2(r_y - v_y\tau) \operatorname{erf}\left(\frac{r_y - v_y\tau}{2\sqrt{D\tau + \sigma^2}}\right) + (a + r_y - v_y\tau) \operatorname{erf}\left(\frac{a + r_y - v_y\tau}{2\sqrt{D\tau + \sigma^2}}\right) \right.$$

$$\left. + (a - r_y + v_y\tau) \operatorname{erf}\left(\frac{a - r_y + v_y\tau}{2\sqrt{D\tau + \sigma^2}}\right) \right)$$

Here $N = \langle C \rangle a^2$ where a is the pixel size in object space, C is the surface concentration, τ is the lagtime, D is diffusion coefficient, v_x and v_y are the velocities in the x and y axes respectively and G_{∞} is the convergence value of the function at long lag times. σ is the standard deviation of the separable Gaussian approximation to the point spread function (PSF) of the microscope in the x - y plane [14, 15].

$$PSF(x, x_0, y, y_0) = PSF(x, x_0) \times PSF(y, y_0) \quad [S2]$$

$$PSF(x, x_0) = \frac{1}{\sigma\sqrt{2\pi}} e^{-\frac{(x-x_0)^2}{2\sigma^2}}$$

where

$$\sigma = \frac{\sigma_0 \lambda_{em}}{NA}$$

λ_{em} is the wavelength of emission and NA is the numerical aperture and σ_0 is a numerical value to be determined by fitting. By setting $r_x = r_y = 0$ in Eq. [S1], the model can be simplified to describe the autocorrelation as in Eq. [S3]. This model has 6 fitting parameters, D , v_x , v_y , N , G_∞ and σ . It can be seen from Eqn. [S3] that autocorrelation is an even function in v_x and v_y . Hence cross-correlations need to be computed to determine the direction of flow. By setting $\sigma = 0$, Eq. [S3] can be simplified into model for autocorrelation as provided in [16, 17].

$$G_{df}(\tau) = G_\infty + \frac{1}{4Na^2} \times \quad [S3]$$

$$\left(\begin{aligned} & \frac{2\sqrt{D\tau + \sigma^2}}{\sqrt{\pi}} \left(e^{-\frac{(a-v_x\tau)^2}{4(D\tau + \sigma^2)}} + e^{-\frac{(a+v_x\tau)^2}{4(D\tau + \sigma^2)}} - 2e^{-\frac{(v_x\tau)^2}{4(D\tau + \sigma^2)}} \right) \\ & - 2(v_x\tau) \operatorname{erf} \left(\frac{v_x\tau}{2\sqrt{(D\tau + \sigma^2)}} \right) \\ & + (a - v_x\tau) \operatorname{erf} \left(\frac{a - v_x\tau}{2\sqrt{(D\tau + \sigma^2)}} \right) + (a + v_x\tau) \operatorname{erf} \left(\frac{a + v_x\tau}{2\sqrt{(D\tau + \sigma^2)}} \right) \end{aligned} \right) \times$$

$$\left(\begin{aligned} & \frac{2\sqrt{D\tau + \sigma^2}}{\sqrt{\pi}} \left(e^{-\frac{(a-v_y\tau)^2}{4(D\tau + \sigma^2)}} + e^{-\frac{(a+v_y\tau)^2}{4(D\tau + \sigma^2)}} - 2e^{-\frac{(v_y\tau)^2}{4(D\tau + \sigma^2)}} \right) \\ & - 2(v_y\tau) \operatorname{erf} \left(\frac{v_y\tau}{2\sqrt{(D\tau + \sigma^2)}} \right) \\ & + (a - v_y\tau) \operatorname{erf} \left(\frac{a - v_y\tau}{2\sqrt{(D\tau + \sigma^2)}} \right) + (a + v_y\tau) \operatorname{erf} \left(\frac{a + v_y\tau}{2\sqrt{(D\tau + \sigma^2)}} \right) \end{aligned} \right)$$

3.2 Expressions for ΔCCF for diffusion and flow

The expression for the cross-correlation function for diffusion separated by r_x along the x-axis can be obtained from Eq. [S1] by setting $v_x = v_y = r_y = 0$ and is an even function in r_x . ΔCCF which is defined as the differences between the forward and the backward correlation, in this case, is $G_{CCF}(r_x, \tau) - G_{CCF}(-r_x, \tau)$. This expression, evaluates to zero on an average.

$$G_{CCF}(r_x, \tau) = G_\infty + \frac{1}{4Na^2} \times \quad [S4]$$

$$\left(\frac{4\sqrt{D\tau + \sigma^2}}{\sqrt{\pi}} \left(e^{\frac{-(a)^2}{4(D\tau + \sigma^2)}} - 1 \right) + (2a) \operatorname{erf} \left(\frac{a}{2\sqrt{D\tau + \sigma^2}} \right) \right) \times$$

$$\left(\frac{2\sqrt{D\tau + \sigma^2}}{\sqrt{\pi}} \left(e^{\frac{-(a+r_x)^2}{4(D\tau + \sigma^2)}} + e^{\frac{-(a-r_x)^2}{4(D\tau + \sigma^2)}} - 2e^{\frac{-r_x^2}{4(D\tau + \sigma^2)}} \right) - 2r_x \operatorname{erf} \left(\frac{r_x}{2\sqrt{D\tau + \sigma^2}} \right) \right)$$

$$+ (a + r_x) \operatorname{erf} \left(\frac{a + r_x}{2\sqrt{D\tau + \sigma^2}} \right) + (a - r_x) \operatorname{erf} \left(\frac{a - r_x}{2\sqrt{D\tau + \sigma^2}} \right)$$

This is not the case when the system exhibits flow where the function is not an even function in r_x as seen from the equation below. By setting $D = r_y = 0$, Eq. [S1] is modified as

$$G_{CCF,f}(\tau) = \frac{1}{2Na^2} \left(\frac{2\sigma}{\sqrt{\pi}} \left(e^{\frac{-(a)^2}{4\sigma^2}} - 1 \right) + a \operatorname{erf} \left(\frac{a}{2\sigma} \right) \right) \times \quad [S5]$$

$$\left(\frac{2\sigma}{\sqrt{\pi}} \left(e^{\frac{-(a+r_x-v_x\tau)^2}{4\sigma^2}} + e^{\frac{-(a-r_x+v_x\tau)^2}{4\sigma^2}} - 2e^{\frac{-(r_x-v_x\tau)^2}{4\sigma^2}} \right) - 2(r_x - v_x\tau) \operatorname{erf} \left(\frac{r_x - v_x\tau}{2\sigma} \right) \right)$$

$$+ (a + r_x - v_x\tau) \operatorname{erf} \left(\frac{a + r_x - v_x\tau}{2\sigma} \right) + (a - r_x + v_x\tau) \operatorname{erf} \left(\frac{a - r_x + v_x\tau}{2\sigma} \right)$$

3.3 Fitting model for SPIM-FCCS

In the case of light sheet of considerable thickness in z direction, the same model was adapted to include the light sheet thickness and is given in [18].

$$G_{df}(\tau) = G_{\infty} + \frac{1}{4Na^2 \sqrt{\pi \left(1 + \frac{D\tau}{\sigma_z^2}\right)}} \times \quad [S6]$$

$$\left(\begin{aligned} & \frac{2\sqrt{D\tau + \sigma^2}}{\sqrt{\pi}} \left(e^{-\frac{(a+r_x-v_x\tau)^2}{4(D\tau + \sigma^2)}} + e^{-\frac{(a-r_x+v_x\tau)^2}{4(D\tau + \sigma^2)}} - 2e^{-\frac{(r_x-v_x\tau)^2}{4(D\tau + \sigma^2)}} \right) \\ & -2(r_x - v_x\tau) \operatorname{erf}\left(\frac{r_x - v_x\tau}{2\sqrt{(D\tau + \sigma^2)}}\right) + (a + r_x - v_x\tau) \operatorname{erf}\left(\frac{a + r_x - v_x\tau}{2\sqrt{(D\tau + \sigma^2)}}\right) \\ & + (a - r_x + v_x\tau) \operatorname{erf}\left(\frac{a - r_x + v_x\tau}{2\sqrt{(D\tau + \sigma^2)}}\right) \\ & \frac{2\sqrt{D\tau + \sigma^2}}{\sqrt{\pi}} \left(e^{-\frac{(a+r_y-v_y\tau)^2}{4(D\tau + \sigma^2)}} + e^{-\frac{(a-r_y+v_y\tau)^2}{4(D\tau + \sigma^2)}} - 2e^{-\frac{(r_y-v_y\tau)^2}{4(D\tau + \sigma^2)}} \right) \\ & -2(r_y - v_y\tau) \operatorname{erf}\left(\frac{r_y - v_y\tau}{2\sqrt{(D\tau + \sigma^2)}}\right) + (a + r_y - v_y\tau) \operatorname{erf}\left(\frac{a + r_y - v_y\tau}{2\sqrt{(D\tau + \sigma^2)}}\right) \\ & + (a - r_y + v_y\tau) \operatorname{erf}\left(\frac{a - r_y + v_y\tau}{2\sqrt{(D\tau + \sigma^2)}}\right) \end{aligned} \right) \times$$

Where $N = 2\langle a^2 \sigma_z^2 \rangle$ where σ_z is defined as the standard deviation of the Gaussian in the z direction. It is to be noted that the definitions of N are different in both the expressions.

$$I(z, m) = \frac{1}{\sigma_z \sqrt{2\pi}} e^{-\frac{(z-m)^2}{2\sigma_z^2}} \quad [S7]$$

This model has 4 fitting parameters; D , v_x , v_y and G_{∞} . The value of σ_0 is fixed to 0.61 and the value of σ_z can be measured [18]. By a similar reasoning, the cross-correlations have to be computed to determine the direction in SPIM-FCCS.

4. Standard deviations for weighted fitting

4.1 Koppel's formula

$$\begin{aligned} \sigma^2(k\Delta\tau) = & \quad [S8] \\ & \frac{1}{nN^2} \left[\frac{(1+g^2(\Delta\tau))(1+g^2(k\Delta\tau))}{(1-g^2(k\Delta\tau))} + 2kg^2(k\Delta\tau) \right] \\ & + \frac{1}{n} \left[\frac{2(1+g^2(k\Delta\tau))}{NF_A} + \frac{1}{F_A^2} \left(1 + \frac{g(k\Delta\tau)}{N} \right) \right] \\ & \forall \{k \in \mathbb{N} \mid 0 \leq k < p\} \\ & g(\Delta\tau) = G(\Delta\tau) - 1 \end{aligned}$$

Subsequently, for the next groups of channels

$$\begin{aligned} \sigma^2(y\Delta\tau) = & \quad [S9] \\ & \frac{1}{\left\lfloor \frac{n}{2^l} \right\rfloor N^2} \left[\frac{(1+g^2(2^l\Delta\tau))(1+g^2(y\Delta\tau))}{(1-g^2(y\Delta\tau))} + 2kg^2(y\Delta\tau) \right] \\ & + \frac{1}{\left\lfloor \frac{n}{2^l} \right\rfloor} \left[\frac{2(1+g^2(y\Delta\tau))}{2^l NF_A} + \frac{\left(1 + \frac{g(y\Delta\tau)}{N} \right)}{2^{2l} \langle F_A \rangle^2} \right] \text{ where } y = 2^l \left(k + \frac{p}{2} + 1 \right) - 1 \\ & \forall \left\{ k, l \in \mathbb{N} \mid \begin{array}{l} 0 \leq k < \frac{p}{2} \\ 1 \leq l < q \end{array} \right\} \end{aligned}$$

4.2 Calculation of $\sigma_{i,data}$ while calculating the mean

$$\begin{aligned} \sigma(k\Delta\tau) = & \quad [S10] \\ & \frac{(n-k) \left(\sum_{i=0}^{n-k-1} F_A^2(i\Delta\tau) F_B^2((i+k)\Delta\tau) - \frac{\left(\sum_{i=0}^{n-k-1} F_A(i\Delta\tau) F_B((i+k)\Delta\tau) \right)^2}{(n-k)} \right)^{\frac{1}{2}}}{\sum_{i=0}^{n-k-1} F_A(i\Delta\tau) \sum_{i=k}^{n-1} F_B(i\Delta\tau)} \\ & \forall \{k \in \mathbb{N} \mid 0 \leq k < p\} \end{aligned}$$

Then, for the groups of channels whose bin widths are in GP, the standard deviation is evaluated by

$$\begin{aligned}
 & \sigma \left(\left(2^l \left(k + \frac{p}{2} + 1 \right) - 1 \right) \Delta \tau \right) \quad [S11] \\
 & = \frac{\left(\left(\left\lfloor \frac{n}{2^l} \right\rfloor - k - \frac{p}{2} \right) \left[\left(\sum_{i=0}^{\left\lfloor \frac{n}{2^l} \right\rfloor - k - \frac{p}{2} - 1} \left(\sum_{j=2^l \times i}^{2^l \times (i+1) - 1} F_A(j \Delta \tau) \right)^2 \sum_{j=2^l \times \left(i + k + \frac{p}{2} \right)}^{2^l \times \left(i + k + \frac{p}{2} + 1 \right) - 1} F_B(j \Delta \tau) \right)^2 \right] \right)^{\frac{1}{2}}}{\left(\left\lfloor \frac{n}{2^l} \right\rfloor - k - \frac{p}{2} \right)} \\
 & \quad - \frac{\left(\left(\left\lfloor \frac{n}{2^l} \right\rfloor - k - \frac{p}{2} \right) \left[\left(\sum_{i=0}^{\left\lfloor \frac{n}{2^l} \right\rfloor - k - \frac{p}{2} - 1} \left(\sum_{j=2^l \times i}^{2^l \times (i+1) - 1} F_A(j \Delta \tau) \right)^2 \sum_{j=2^l \times \left(i + k + \frac{p}{2} \right)}^{2^l \times \left(i + k + \frac{p}{2} + 1 \right) - 1} F_B(j \Delta \tau) \right)^2 \right] \right)^{\frac{1}{2}}}{\left(\left\lfloor \frac{n}{2^l} \right\rfloor - k - \frac{p}{2} \right)} \\
 & \quad \forall \left\{ k, l \in \mathbb{N} \left| \begin{array}{l} 0 \leq k < \frac{p}{2} \\ 1 \leq l < q \end{array} \right. \right\}
 \end{aligned}$$

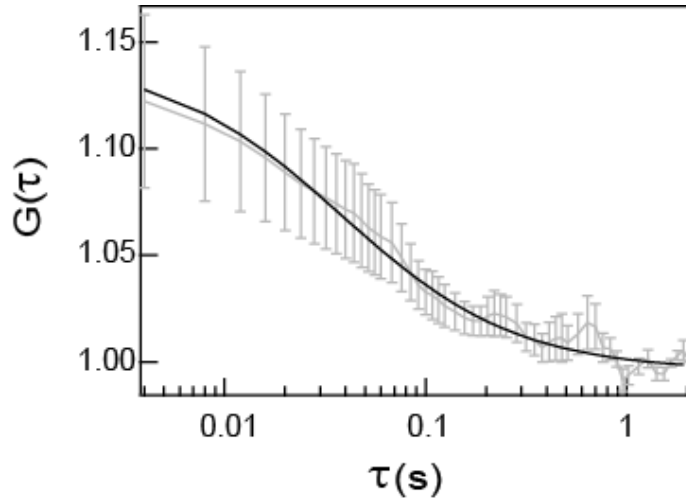


Fig. S4: This is a representative example of weighted fitting. The original stack was split into 10 smaller stacks. The average and standard deviation of the values were obtained from these 10 datasets.

5. Materials and Methods

5.1 Reagents and Protocols

The lipids used in ITIRFCS measurements were Palmitoyl-2-oleoyl-sn-glycero-3-phosphocholine (POPC), 1-Palmitoyl-2-Oleoyl-sn-Glycero-3-[Phospho-*rac*-(1-glycerol)] (Sodium Salt) (POPG) and 1,2-dipalmitoyl-sn-glycerol-3-phosphoethanolamine-N-(lissamine rhodamine B sulfonyl) ammonium salt (Rho-PE) obtained from Avanti Polar lipids (Alabaster, AL). A detailed protocol of the preparation of the lipid bilayers is given in [13]. The details of the quantum dots, the microscope stage used to demonstrate flow processes are given elsewhere [13]. IVA-FCS was performed using fluorescent beads (0.17 μm diameter yellow-green carboxylate modified microspheres $\lambda_{exc} = 505 \text{ nm}$, $\lambda_{em} = 515 \text{ nm}$, PS SpeckTM) obtained from Molecular Probes (Eugene, OR, USA). The preparation of zebrafish embryos and fluorescent beads for measurement for SPIM-FCS are described in [18]. The growth condition of CHO cells, the plasmid sequence and the transfection protocols for EGFR-EGFP are given elsewhere [19].

5.2 Instrumentation

ITIR-FCS and IVA-FCS measurements were performed using an objective-type total internal reflection fluorescence microscope (TIRFM) built using an inverted epifluorescence microscope (IX-71, Olympus) with a high NA oil-immersion objective (100X/1.45) (Olympus, Singapore). Dual color air-cooled ion LASER source ($\lambda_{em} = 514 \text{ nm}$, 185-F02, Spectra-Physics, Mountain View, CA, USA) was used to excite the fluorophores.. The EMCCD camera (Andor iXON 860, 128x128 pixels) was mounted on the side-port of the microscope. Andor Solis (Ver: 4.9.30000.0) was used as the image acquisition software. Each pixel measures $24 \times 24 \mu\text{m}^2$ on the chip and hence $a = 240 \text{ nm}$. The measurements were carried out with a $\Delta\tau = 0.56 \text{ ms}$ for a ROI of 21×21 pixels. The details of the another instrument used to perform ITIR-FCS are described in [13]. The details of the SPIM-FCS instrument are provided in [18].

6. Bleach correction

One of the most common problems encountered in camera based FCS is bleaching. The irreversible loss in fluorescence intensity observed during acquisition times is referred to as bleaching. At very high intensity decay rates, the correlation curves are dominated by bleaching instead of underlying fluctuations in the system. The easiest way to identify bleaching is by visual inspection of intensity trace which shows a gradual loss in fluorescence. Bleaching is evident in autocorrelations as well. Autocorrelation curves affected by bleaching are characterized by non-convergence of the curves. The fitted value of G_{∞} is not close to the expected theoretical value of 1. Upon fitting, the diffusion coefficients retrieved for curves affected by bleaching is around 2 orders of magnitude lower than the expected value. It is necessary to correct the affected intensity traces before the calculation of autocorrelation [20]. It is assumed that the decay of fluorescence can be modeled by a bi-exponential curve. Upon fitting, the raw-data is multiplied by the ratio of the value of the fitted curve at that instant to that of the initial value of the fitted curve to obtain the corrected data. The corrected data is used further for the calculation of correlation.

$$F(t) = F_0 + A_1 e^{-\left(\frac{t-t_0}{T_1}\right)} + A_2 e^{-\left(\frac{t-t_0}{T_2}\right)} \quad [\text{S12}]$$

Where $F(t)$ is the decaying fluorescent trace, t_0 is the acquisition time of the first frame to be fitted. T_1 and T_2 are the fluorescence decay constants. F_0 , A_1 , A_2 , T_1 and T_2 are fitting parameters.

7. Curve Fitting in Igor Pro

This program provides an option to the user to perform curve fitting using Igor Pro. It makes use of FuncFit command in Igor Pro. The FuncFit command provides a variety of options to check the status of the fit. V_FitQuitReason is a variable defined in Igor which is set to zero on proper convergence. After the iterations, if V_FitQuitReason equals 0, the fitted parameter is stored; else it is stored as NAN (Not a Number) indicating a failed fit. The bleach correction fitting is implemented in Igor Pro.

8. Representative histograms of D and N

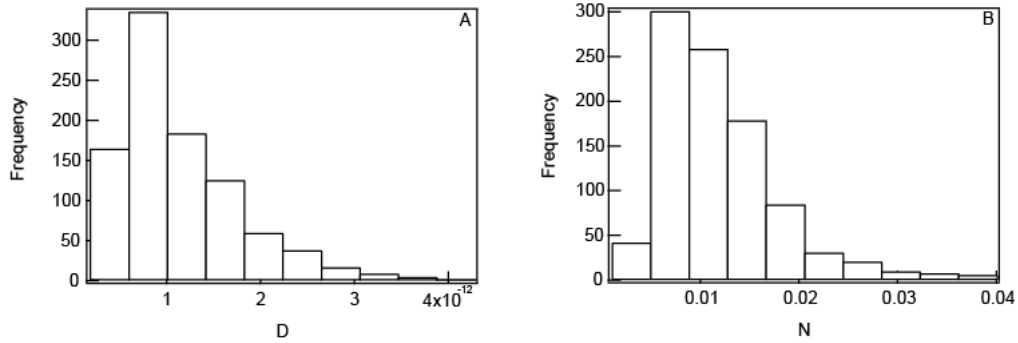


Fig.S5: A histogram of the D and N values of the data described in Figs. 2 G-I is shown in A and B respectively. Fluorescent beads were measured using IVA-FCS in this example.

9. General guidelines on Imaging FCS measurements

In this section, a few practical guidelines on S/N ratio, pixel size, binning and frame rate of the camera are provided for the interested users of Imaging FCS.

9.1 S/N ratio

Any data recorded with a camera has a background which is due to the offset of the A/D converter, the autofluorescence of the sample, the excitation laser leakage and the ambient light in the room [21]. The background counts needs to be subtracted before the calculation of the autocorrelation. By experience, we would recommend that the photon counts in the signal needs to be at least 1.5 times that of the background.

9.2 Photobleaching

The three illumination schemes used for imaging FCS, total internal reflection, variable angle and single plane illumination, illuminate only those regions in the sample which are being measured. As a result, there is reduced photobleaching compared to confocal FCS setups. As a result of reduced phototoxicity, measurements can be performed for longer times, it is also

to be noted that, in SPIM-FCS, the light source is used more effectively and hence SPIM-FCS can be performed at low laser powers leading to less photobleaching [18].

9.3 Pixel Size and Binning

The pixel size on the object space is determined by the physical size of the pixel and the magnification of the detection objective. The physical size of the pixel is in turn dependent on the image capture region size of the chip and the number of pixels in the chip. The optimum binning to be used for the system depends on the pixel size in the object space. The images collected on the chip are diffraction limited. Hence, a pixel size smaller than the diffraction limit, leads only to empty magnification. For cases, where the pixel size is smaller than the diffraction limit, it can be binned to reach the diffraction limit. A detailed discussion of binning for ITIR-FCS and SPIM-FCS is available at [13, 16, 18]. It has already been shown that the diffusion coefficient obtained is independent of the binning used in Imaging FCS [16, 18].

There are two ways to carry out binning, software and hardware binning. The advantage of using software binning is that, the raw data can be binned to yield greater pixel sizes of any size by performing the corresponding binning. But, the drawback is that, in the case of software binning, the binned pixels contains the sum of readout noises of all its constituent pixels before binning. This drawback is observed in a sCMOS and is not an issue in the case of EMCCD. In the case of hardware binning, the readout noise is reduced and the data file occupies less storage space in the memory. While binning, it also has to be kept in mind that, a binned data has less number of correlations to average and the binning leads to a loss in spatial resolution.

9.4 Readout Speed of the Camera

The rule of thumb is that measurements need to be about 10 times faster than the fastest process to be observed by Imaging FCS. The readout speed of the camera is influenced by the size and shape of the region of interest. Reading a sub-array of the chip of the camera increases the readout of the camera. Presently, we have measured up to 2000 fps on a square region of 20 pixels. A lipid bilayer was prepared and the same sample was measured for a wide variety of readout speeds from 250 to 2000 fps and there was only a 10% change in D's extracted from these datasets [data not shown]. A 1 way ANOVA revealed that the differences between D obtained at frame rates of 250, 500 and 1000 are not statistically significant at the 0.2% level. It should also be remembered that data collected using faster frame rates are noisier than those collected with slower frame rates. In the case of a lipid bilayer, the standard deviation of the D's is 50% of the mean value in the case of 2000 fps, whereas the standard deviation of the D's are 30% of the mean at slower frame rates (250-1000 fps).

10. Comparison of Imaging FCS with other fluorescent methods

ITIR-FCS has been systematically compared with other fluorescent techniques like Fluorescent Recovery After Photobleaching (FRAP), confocal FCS and Single Particle Tracking (SPT) in [16]. In general, the diffusion coefficients obtained from ITIR-FCS are comparable with those obtained from FRAP. The Ds obtained from confocal FCS are larger than those from ITIR-FCS. This is due to the limited time resolution of the state of the art cameras today. SPT shows a wider range of D's when compared to that of ITIR-FCS. Using z-scan FCS or two-focus (2f) FCS, both of which are calibration free methods, the diffusion coefficients of lipids diffusing on a bilayer was determined to be 2–5 $\mu\text{m}^2/\text{s}$ [22-24]. The

values obtained from ITIR-FCS also fall in the same range [13]. In the case of measurements on biological systems, it was demonstrated using ITIR-FCS that there is a 2-3 times increase in D of raft markers upon treatment with cholesterol depleting or/and actin depolymerizing agents. The same trend has been observed by other techniques as well. Image Correlation Spectroscopy revealed that upon cholesterol depletion, D increased by a factor of 2 for GPI anchored proteins [25]. Using FRAP, it was demonstrated that cholesterol removal or cytoskeletal disruption led to a 2-3 times increase in increase in D for Dopamine transporter protein [26]. The accuracy of the D 's extracted out of SPIM-FCS were demonstrated by the authors using different experiments on fluorescent beads [18]. In the case of IVA-FCS, the diffusion coefficient of beads reported here, the values are similar to those obtained from SPIM-FCS [18]. In conclusion, all the Imaging FCS methods retrieve diffusion coefficients which are comparable with expected values and those obtained from other techniques.